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In the claims:

1. (Currently Amended) A magnetic resonance imaging system comprising:

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at least one superconducting magnet generating a static magnetic field;

- a gradient coil assembly with an associated patient bore enclosure comprising;
 - at least one gradient coil generating at least one gradient magnetic field; and
 - at least one static field-shaping coil residing between said at least one superconducting magnet gradient coil and said patient bore enclosure and supplementing said static magnetic field.
- 2. (Original) A system as in claim 1 wherein said at least one superconducting magnet resides within a cryostat having at least one thermal shield, said at least one static field-shaping coil resides between said at least one thermal shield and said patient bore enclosure.
- 3. (Original) A system as in claim 1 further comprising at least one gradient shield coil compensating for pulse sequences generated within the magnetic resonance imaging system.
- 4. (Original) A system as in claim 3 wherein said at least one gradient shield coil resides between said at least one superconducting magnet and said gradient coil assembly.
- 5. (Original) A system as in claim 3 wherein said at least one static field-shaping coil resides between said at least one gradient shield coil and said patient bore enclosure.

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- 6. (Original) A system as in claim 3 wherein said gradient coil assembly comprises said at least one gradient shield coil.
- 7. (Original) A system as in claim 1 further comprising a static field-shaping coil housing residing within a magnet structure of the magnetic resonance imaging system, said at least one static field-shaping coil residing within said static field-shaping coil housing.
- 8. (Original) A system as in claim 7 wherein said static field-shaping coil housing is formed of a material that prevents induction of eddy currents therein.
- 9. (Original) A system as in claim 7 wherein said static field-shaping coil housing is formed of a composite material.
- 10. (Original) A system as in claim 7 wherein said static field-shaping coil housing comprises a coolant.
- 11. (Original) A system as in claim 10 wherein said coolant is cooled via a cryocooler.
- 12. (Original) A system as in claim 1 wherein the magnetic resonance imaging system is of a cylindrical or open architecture design.
- 13. (Original) A system as in claim 1 wherein said at least one superconducting magnet comprises at least one low temperature superconductor.

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- A system as in claim 1 wherein said at least one (Original) 14. temperature superconducting magnet comprises at least one high superconductor.
- A system as in claim 1 wherein said at least one static **15.** (Original) field-shaping coil comprises at least one low temperature superconductor.
- A system as in claim 1 wherein said at least one static (Original) 16. field-shaping coil comprises at least one high temperature superconductor.
- A system as in claim 1 wherein said at least one static **17.** (Original) field-shaping coil is unshielded from said at least one gradient magnetic field.
- A system as in claim 1 wherein said at least one static 18. (Original) field-shaping coil is inductively isolated from said at least one gradient coil assembly.
- A system as in claim 1 wherein said at least one static **19.** (Original) field-shaping coil is cooled using at least one of a cryogen bath, conduction, or convection.
- A system as in claim 1 wherein said at least one static 20. (Original) field-shaping coil is cooled via a coolant selected from at least one of helium, nitrogen, hydrogen, or neon.
- A system as in claim 1 wherein said at least one static (Original) 21. field-shaping coil is approximately a factor of ten smaller than said at least one superconducting magnet.

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A system as in claim 1 wherein at least one of said at (Original) 22. least one static field-shaping coil is replaced with an iron ring.

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- A system as in claim 1 wherein said at least one (Original) 23. superconducting magnet resides at least partially within a first former and said at least one static field-shaping coil resides at least partially within a second former.
- A magnetic resonance imaging system (Currently Amended) 24. comprising:

at least one superconducting magnet generating a static magnetic field;

- at least one gradient shield coil compensating for pulse sequences generated within the magnetic resonance imaging system;
- a gradient coil assembly with an associated patient bore enclosure comprising;
 - at least one gradient coil generating at least one gradient magnetic field; and
 - at least one supplemental static field-shaping coil residing between said at least one superconducting magnet gradient coil and said patient bore enclosure and increasing strength of said static magnetic field.
- A system as in claim 24 wherein said at least one (Original) 25. gradient shield coil resides between said at least one superconducting magnet and said gradient coil assembly.
- A magnetic resonance imaging system (Currently Amended) 26. comprising:
 - at least one superconducting magnet generating a static magnetic field;
- at least one gradient shield coil compensating for pulse sequences generated within the magnetic resonance imaging system;

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a gradient coil assembly with an associated patient bore enclosure comprising;

at least one gradient coil generating at least one gradient magnetic field in the patient bore; and

said at least one superconducting magnet gradient coil and said patient bore enclosure, said at least one supplemental static field-shaping coil being unshielded from said at least one gradient magnetic field and increasing strength of said static magnetic field.

27. (Original) A system as in claim 26 wherein said at least one gradient shield coil resides between said at least one superconducting magnet and said gradient coil assembly.